

**IHDE**DENTAL 

**NO-ITIS<sup>®</sup> LASER** DIE NEUE  
**OBERFLÄCHEN**  
GENERATION



Firmengebäude und Produktionsstätte von  
**Dr. Ihde Dental AG** in Gommiswald / Schweiz



IHR INTERESSE IST UNSER ANTRIEB

# NO-ITIS® LASER

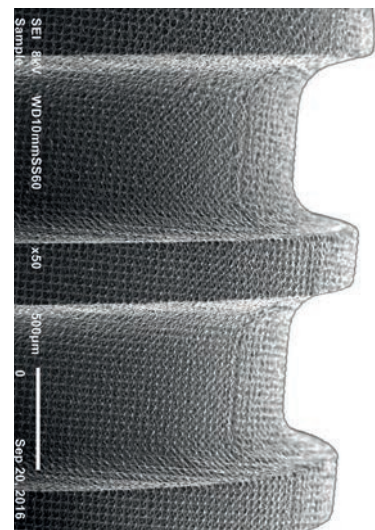
## DIE NEUE OBERFLÄCHENGENERATION

Die neue Oberflächenbeschichtung der Implantate von Dr. Ihde Dental AG erfolgt mit der neuesten Generation von Industrierobotern für die Laserablation. Diese neue, hochpräzise Technologie ermöglicht es, durch ein Netz von symmetrisch verteilten halbkugelförmigen mikrometergroßen Poren von definierter konstanter Größe und Form eine raue Implantatoberfläche zu erzeugen.

Dadurch erhalten wir eine adäquatere Topographie, welche die besten Voraussetzungen für die Osseointegration des Implantats bietet. Gleichzeitig verhält sie sich auf (zellulärer) Mikrometerebene wie eine glatte Oberfläche. Dies bedeutet: Obgleich Knochen gut an diese Oberfläche anwächst, ist die Adhäsion von Bakterien auf dieser Oberfläche signifikant reduziert.

**NO-ITIS® LASER**  
EINE GLATTE OBERFLÄCHE,  
DIE IN KONTAKT MIT DEM  
KNOCHEN WIE EINE RAUE  
OBERFLÄCHE WIRKT

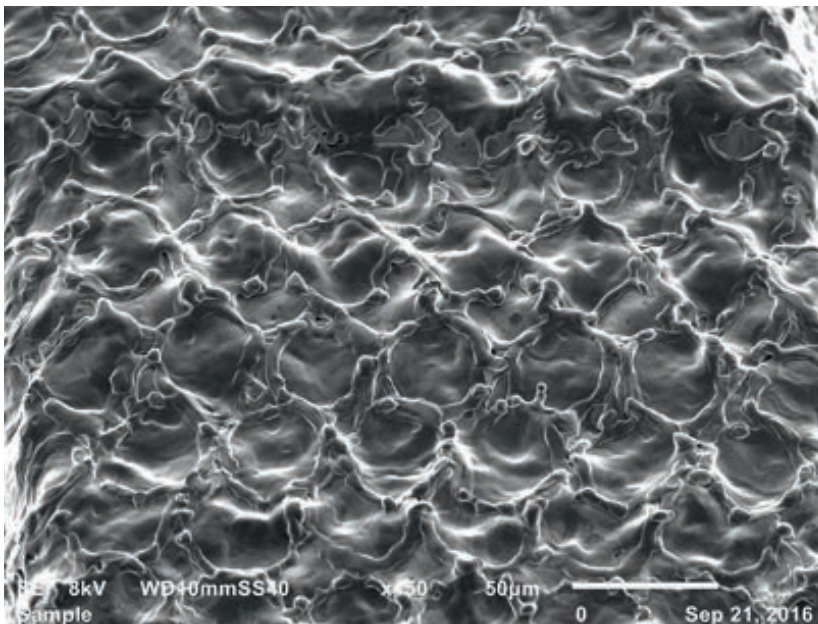
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In den 1990er Jahren wurden raue Oberflächen bei Zahnimplantaten zunehmend beliebter, ohne dass man dabei das Risiko der bakteriellen Adhäsion berücksichtigte. Das hatte das Auftreten einer ganz neuen Krankheit, der Peri-Implantitis, zur Folge, die das Überleben der Implantate langfristig stark beeinträchtigt und damit eine langwierige und kostspielige Neubehandlung des Patienten erforderlich macht. Solche Oberflächen sind nicht patientengerecht!

Der Einsatz der von uns entwickelten Lasertechnologie ermöglicht es, eine exakt definierte Mikromorphologie auf der behandelten Oberfläche zu schaffen, ohne Rückstände zu hinterlassen und ohne die Eigenschaften oder die Zusammensetzung des Titans zu verändern. Es entsteht ein Netz von hochperfekten Hohlräumen – was deren halbkugelförmige Form selbst betrifft wie auch deren Abmessungen (20–30  $\mu\text{m}$ ), den Abstand und die Verteilung. Die Oberfläche dieser Hohlräume sowie die durch die Laserablation gebildeten Retentionen sind jedoch aus Sicht der Bakterien glatt, eine Eigenschaft, bei der man davon ausgeht, dass sie das Implantat resistenter gegen eine Besiedelung durch Bakterien macht. Diese Eigenschaft könnte auch die Häufigkeit von Peri-Implantitis radikal verringern. Im Kontakt mit dem Knochen verhält sich die per Laserablation gestaltete Oberfläche jedoch wie eine raue Oberfläche. Raue Implantate (z. B. KOS<sup>®</sup>, Hexacone<sup>®</sup>) und glatte Implantate (z.B. BCS<sup>®</sup>, BECES<sup>®</sup>, GBC<sup>®</sup>) weisen daher die gleiche Wiederfindungsrate auf.

## **NO-ITIS<sup>®</sup> LASER** DIE OBERFLÄCHE, DIE DIE ÜBERLEBENSRATE ERHÖHT



Rauigkeit (Ra)	Definition
$\leq 0,4 \mu\text{m}$	Glatt
0,5 - 1,0 $\mu\text{m}$	Maschinenglatt
1,0 - 2,0 $\mu\text{m}$	Mässig rau
$> 2,0 \mu\text{m}$	Rau

Rauigkeit (Ra)	No-Itis <sup>®</sup> Laser
0,9 $\mu\text{m}$	Glatt

Nach der Klassifizierung der Oberflächenrauheit von Albrektsson und Wenneberg würde der Ra-Wert einer mässig rauhen Oberfläche entsprechen, obwohl unsere gelaserte Oberfläche tatsächlich die Eigenschaften und viele der Vorteile einer glatten Implantatoberfläche aufweist.

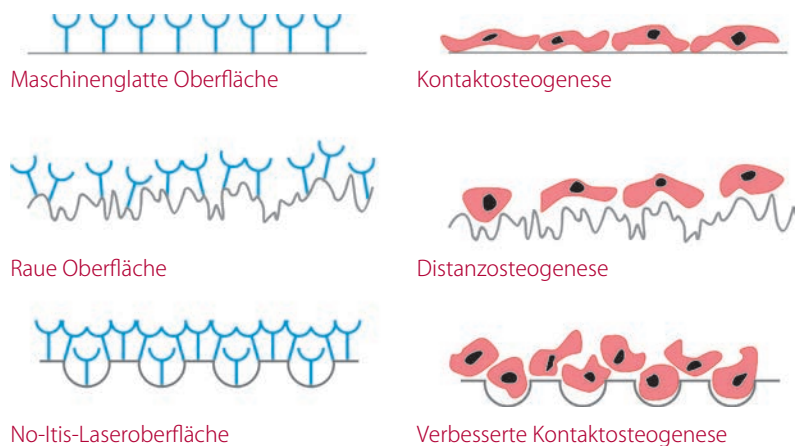
## NO-ITIS® LASER

DIE FORTSCHRITTLICHSTE  
OBERFLÄCHE – EIN WICHTIGER  
ANSATZ ZUR LÖSUNG DES  
PERI-IMPLANTITIS PROBLEMS,  
UND ZUM LANGFRISTIGEN  
ERHALT DER OSSEOINTEGRATION

Die NO-ITIS® LASER-Oberfläche ermöglicht die Adhäsion eines gleichmäßigen und erweiterten Fibringerinnsels, das dann die Bildung von Geflechtknochen bewirkt. Die Verteilung und die Größe der Konkavitäten begünstigen die Anpassung und Aktivität der Osteoblasten und fördern eine effektive Osseointegration.

### STABILES FIBRINETZ

Bei NO-ITIS® LASER wie auch bei einer traditionellen rauhen Oberfläche haften Fibrinfilamente fast ausschließlich an den erhabenen Teilen der Oberfläche an und bilden Brücken zwischen diesen (Distanzosteogenese). Auf der NO-ITIS® LASER-Oberfläche bildet das Fibrin ein gut entwickeltes und wohldefiniertes Gitternetz auch innerhalb der Hohlräume aus, was die Besiedlung durch osteogene Zellen direkt auf der Oberfläche des Implantats begünstigt (Kontaktosteogenese).



## NO-ITIS® LASER

EINE EINZIGARTIGE  
OBERFLÄCHE

### MAXIMALE KONTAKTOSTEOGENESE

Dank der guten Zelladhäsion kann sich auf der vom NO-ITIS® LASER geschaffenen Oberfläche ein normales Fibrinnetz bilden, anpassen und erweitern.

Dieser Prozess aktiviert die Bildung von osteonalem Knochen, auch in direktem Kontakt mit dem Implantat.

## SCHNELLE OSSEOINTEGRATION

Die perfekte symmetrische und reproduzierbare Topographie der **NO-ITIS® LASER**-Oberfläche zieht eine größere Anzahl von osteogenen Zellen an, die sich stabil anlagern und auf der Oberfläche des Implantats gleichmäßig vermehren können. Dieser Prozess aktiviert die Bildung von Knochen in direktem Kontakt mit dem Implantat, was zu einer dynamischeren und günstigeren Osseointegration mit mehr Kontakt zwischen Knochen und Implantat führt und ein echtes Knochen-Engineering ermöglicht.

- Glatte Struktur der Implantatoberfläche
- Geringere bakterielle Adhäsion

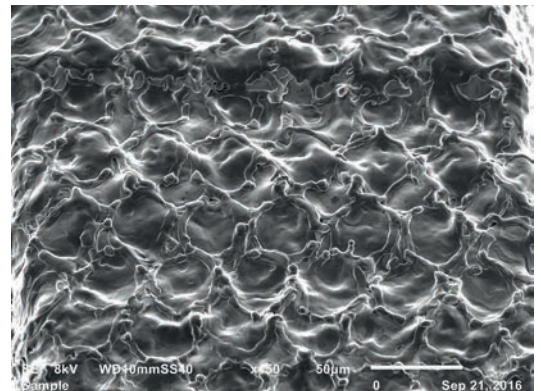
### ➔ GERINGERES INFEKTIONSRISIKO

- Vermehrte Adhäsion von Fibrin
- Mehr Kontaktosteogenese auf einer grösseren Oberfläche

### ➔ PERFEKTE OSSEOINTEGRATION

## NO-ITIS® LASER – EINE REINE OBERFLÄCHE

Im Gegensatz zu Standardoberflächen (durch Sandstrahlen und Ätzen oder Sandstrahlen und Anodisieren) haben die Implantate mit **NO-ITIS® LASER** eine völlig reine Oberfläche ohne Rückstände und Verunreinigungen. Durch diesen modernen Herstellungsprozess kommen grundsätzlich keine Rückstände von Strahlpartikeln oder Spuren der beim Ätzprozess verwendeten Chemikalien (Säuren) oder der Anodisierung (Oxide) in Kontakt mit dem Implantat. Durch den Verzicht auf die Anodisierung entfällt das Risiko, dass sich die oberste Materiallage auf dem eingefärbten Implantat mechanisch löst.



## NO-ITIS® LASER – DIE IDEALE FLÄCHE FÜR KNOCHENKONTAKT

Die absolute Reinheit von **NO-ITIS® LASER** ermöglicht es, die enossale Implantatoberfläche zu vergrößern, ohne die Nachteile herkömmlicher Verfahren zur Oberflächenaufräumung in Kauf nehmen zu müssen.

## NO-ITIS® LASER DIE IDEALE OBERFLÄCHE FÜR SOFORT- UND FRÜHBELASTUNG

## NO-ITIS® LASER EINE REINE OBERFLÄCHE

## NO-ITIS® LASER LITERATUR

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## ORIGINAL ARTICLE



# A comparative study on the microstructural and antibacterial properties of Laser - textured and SLA dental implants.

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## ABSTRACT

**Objective:** To compare the structural and antibacterial properties of a Laser - treated commercial dental implant (No-Itis®) with those of a traditional sandblasted and acid-etched (SLA) implant. **Materials and Methods:** Surface topography and elemental composition of the implant surfaces were analyzed by using scanning electron microscopy (SEM) coupled to dispersive X - ray spectrometry (EDX). The antibacterial properties of the implants were tested against *Aggregatibacter actinomycetemcomitans*. Protein adsorption capacity and bioactivity in simulated body fluid (SBF) of the implant surfaces were also analyzed. **Results:** The Laser - treated implant presents a topography constituted by smooth and uniform concavities of ~ 30 µm in diameter, free of Laser - induced alterations, and impurity elements. The Laser - textured surface demonstrated to significantly ( $p = 0.0132$ ) reduce by up to around 61% the bacterial growth as compared with the SLA implant, which was found to be associated to a reduced adhesion of proteins on the Laser surface. No apatite - related mineral deposits were detected on the SBF - incubated surfaces. **Conclusion:** The smooth Laser - designed surface exhibits an antimicrobial effect that decreases the growth of bacterial biofilm on its surface, which could contribute to reduce the risk of peri-implantitis.

## KEY WORDS

Laser - textured implants; Peri-implantitis; Antimicrobial surfaces.

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## INTRODUCTION

The success of oral rehabilitation using titanium dental implants is largely dependent on the degree of osseointegration at the metal-bone interface as well as the management of peri-implant infections. In this respect several surface modification techniques of titanium implants have been used as strategy to improve the osseointegration properties and prevent infections. Peri-implantitis is the inflammatory disease marked by bacterial infection and the destructive process affecting the soft and hard tissues around osseointegrated implants, leading to the loss of supporting bone<sup>(1,2)</sup>. To reduce the biofilm formation on implant surface, antibacterial coatings loaded with antibiotics<sup>(3)</sup>, chlorhexidine<sup>(4)</sup>, or silver nanoparticles<sup>(5)</sup> have been explored. Other approach consists in the design of titanium implants with different surface textures and topographies. Reduced roughness and surface free energy on implants has shown a positive correlation with the inhibition of bacterial adhesion<sup>(6)</sup>. Thus, different techniques are studied and used to fabricate titanium dental implants with controlled texture including smooth-machined, sand-blasted, acid-etched, and plasma-sprayed surfaces. Laser melt and modify the texture of titanium implants, producing extremely pure, ordered, and uniform surfaces<sup>(7,8)</sup>. Laser texturing replaces a random process (e.g., blasting, etching) with a digital one. Pulses of laser light allow a titanium implant surface to be structured with a precise, repeatable pattern and enables both product designers and manufacturers to design in and meet more exacting specifications for roughness. Currently, dental implants with a robot-manipulated laser surfaces are being introduced to the market<sup>(9)</sup>. Laser-designed surfaces have been proposed to improve the mechanical, chemical, and biological properties of dental implants. Surface topographies may promote cell attachment and differentiation, thus improving the osseointegration properties<sup>(10)</sup>. Also, smoother surfaces produced by Laser treatment have been proposed to reduce the biofilm formation and consequently decrease the risk of peri-implantitis<sup>(11)</sup>. However, scant evidence exists on the antimicrobial properties of Laser-textured implants against peri-implant pathogens as well as comparative studies with irregular surfaces produced through conventional surface treatments.

In this work, the structural, compositional, and antibacterial properties of a Laser-treated commercial implant are systematically compared with that of a sandblasted and acid-etched (SLA) implant. Antibacterial properties are assessed against *Aggregatibacter actinomycetemcomitans*, a representative peri-implant bacterium<sup>(12)</sup>.

## MATERIALS AND METHODS

The current work corresponds to a quantitative, qualitative, and comparative *in vitro* experimental study.

### Surface characterization of dental implants.

Single piece dental implants (Ihde Dental AG, Switzerland) fabricated with titanium alloy grade 5 (Ti6Al4V-ELI) were studied. Laser-textured (No-Itis®) (Laser) and traditional double - sandblasted/acid-etched (SLA) implants were compared. The dental implants had an endossal implant thread of 3.2/3.7 mm and endossal length of 15 mm.

Surface topography of implants was analyzed by scanning electron microscopy (SEM) in a JEOL JSM-IT300LV microscope. Representative SEM images were acquired at 30, 120, 350, and 800 X of magnification with an accelerating voltage of 20 kV. Atomic-resolution compositional mapping on the implant surfaces was performed by energy dispersive X-ray spectrometry (EDX) (Aztec EDS, Oxford Instruments) coupled to the SEM microscope. The surfaces of a total of five implants of each type were analyzed, and representative SEM images of them are presented.

### Antibacterial activity

The growth of *Aggregatibacter actinomycetemcomitans* serotype b (ATCC® 43718™) was assessed on the implant surfaces. Each sterilized implant was vertically placed in tubes with 990 µL of fresh Brain Heart Infusion (BHI) and 10 µL of the inoculum (adjusted to 2 McFarland standard), and incubated for 48 hours in a 5% CO<sub>2</sub> atmosphere at 37 °C. After the incubation period, the implants were removed from the growth medium and immersed into a 1% Tween 80 saline solution to remove the adherent bacteria. The dilutions taken from the bacterial suspensions were plated onto BHI agar and incubated for 48 h at 37 °C. After that, the colonies were counted and the colony forming units per implant surface (CFU/mm<sup>2</sup>) were calculated.

Bacterial biofilm formed on each implant surface was examined by SEM microscopy. After incubation period, adherent bacteria were fixed by immersing the implants in 2.5% glutaraldehyde, then dehydrated in ethanol series, dried in supercritical CO<sub>2</sub> (Tousimis, Autosamdri-815) and gold coated prior to SEM imaging.

### Protein adsorption

The protein adsorption capacity of the dental implant surfaces was determined by using bovine serum albumin (Merck) as model protein.



1.5 mL of buffered solution (pH 7.4,  $K_2HPO_4/KH_2PO_4$  100 mM) containing 0.4 mg/mL of protein was contacted with each implant vertically placed in a 24-well cell culture plate. After 6 h of incubation at 37°C, the implants were removed from the protein solution and washed with phosphate buffer to remove the nonadherent proteins. Then, the adhered proteins were extracted from the implant surfaces by incubating with 1.5 mL of 2% sodium dodecyl sulfate solution for 12 h at 37°C. The concentration of extracted protein was measured using the colorimetric Micro Bicinchoninic Acid Assay Kit (Thermo Scientific).

#### Surface bioactivity assay

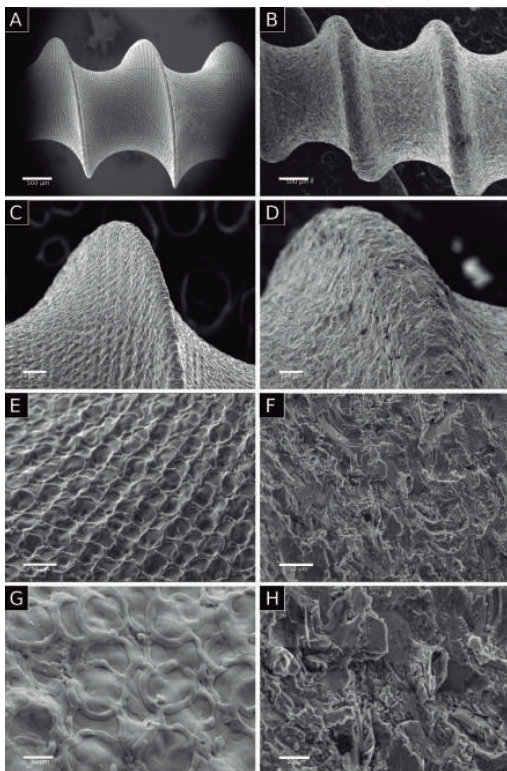
The ability of implant surface to form bone-like apatite in acellular simulated body fluid (SBF) was evaluated according to ISO/FDIS 23317:2007 (E). The Kokubo's SBF solution pH 7.4 was prepared with the ionic composition and procedure described elsewhere<sup>(13)</sup>. The implant samples were individually immersed in 50 mL of SBF in polyethylene bottles at 36.5 °C in a thermostatic shaking water bath. After 28 days of incubation, the implants were removed from SBF, immersed in distilled water for 3 min, and dried at 60 °C. The apatite mineralized on the implant surfaces was analyzed by SEM and EDX compositional measurements.

#### Statistical analysis

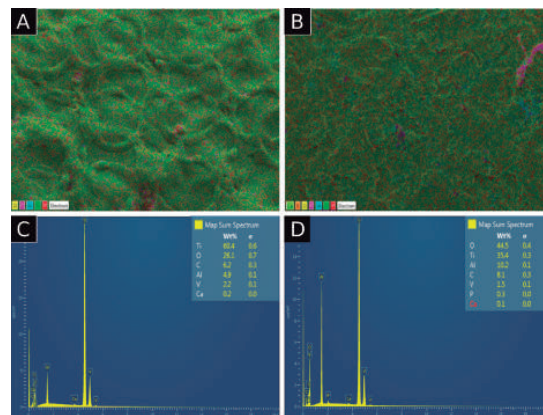
Statistical analysis of colony forming unit counting data was carried out by using GraphPad prism 6 (GraphPad Software, San Diego, CA). One-way analysis of variance with post hoc multiple comparisons (Tukey's test) was performed on a minimum of n=5 (significance level,  $P < 0.05$ ).

## RESULTS

Fig. 1 presents the SEM images of the dental implant surfaces acquired with different magnification. The Laser-treated implant exhibits a topography constituted by uniform and circular concavities of ~ 30 µm in diameter and ~ 2 µm of border width, which are regularly distributed on the entire implant surface. The inner and outer area of the concavities present a smooth texture and free of porosity or other Laser-induced alterations. In contrast, the SLA implant exhibits a disorganized, rough, and uneven surface. EDX elemental analysis (Fig. 2) confirmed the presence of Ti, Al, V and O as main components of the oxidized Ti6Al4V implant surfaces. C, Ca, and P were detected as minor or trace components of the surfaces.

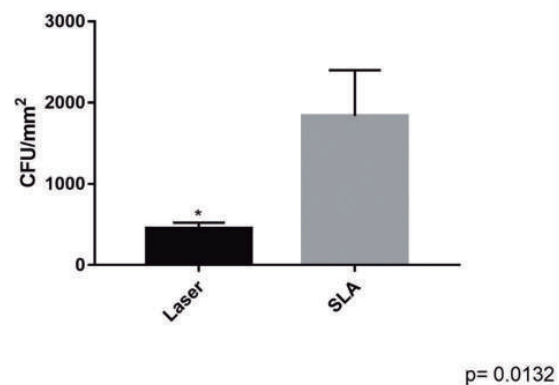


**Figure 1.** SEM images of titanium dental implant surfaces of Laser (A, B) and SLA (C, D) at 30X of magnification and Laser (E, F) and SLA (G, H) at 800X of magnification.



**Figure 2.** EDX compositional analysis of the dental implant surfaces. EDX elemental distribution maps on the Laser (A) and SLA (B) implant surfaces. EDX spectra showing the weight percentage values of present elements on the Laser (C) and SLA (D) implant surfaces.

The survival of *A. actinomycetemcomitans* biofilm grown per area of implant surface is shown Fig. 3. The results show that bacterial survival is significantly ( $p = 0.0132$ ) reduced by up to around 61% on the Laser-treated implant surface as compared with the traditional SLA implant surface. SEM images (Fig. 4) confirm a substantially lower amount of bacterial biofilm developed on the Laser implant. Abundant microcolonies anchored to the surface and apparently embedded in their exopolysaccharide matrix<sup>(14)</sup> can be observed on the SLA implant (white arrows, Fig. 4h).



**Figure 3.** Survival of *A. actinomycetemcomitans* biofilm grown per area of implant surface after 48 hours of incubation using a 2 McFarland standard. Each value is mean ± sd (n=5). \* indicates  $p < 0.05$ .

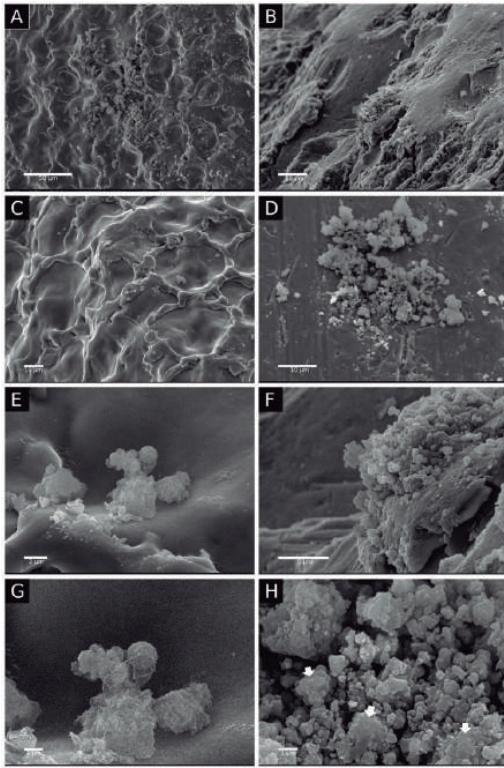
The albumin protein adsorption capacities for the Laser and SLA implant surfaces were 390 ng/mm<sup>2</sup> and 540 ng/mm<sup>2</sup>, respectively.

Fig. 5 shows SEM images and EDX compositional mapping of the implant surfaces after 28 days of immersion in SBF. Although the implant textures appear to be slightly modified, no apatite deposits or related minerals were detected on the surfaces. The Ca and P contents measured by EDX were not significant.

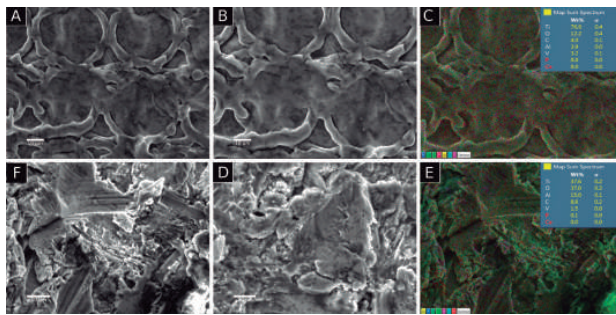
## DISCUSSION

The topography, chemical composition, and bioactive properties of the Laser-textured implant surface was analyzed and systematically compared with that of a traditional SLA implant. The results confirm that the Laser implant presents a highly regular and smooth surface according to the information provided by the manufacturer, which contrast with the disorganized and rough surface of the SLA implant. Laser treatment also showed to produce topographical modifications of the implant surface without altering its surface chemical composition.

Microbiological assays demonstrated that the Laser implant exhibits



**Figure 4.** SEM images of *A. actinomycetemcomitans* biofilm grown on Laser implant surface at 500X (A), 1,000X (C), 6,000X (G) and 10,000X (E) of magnification and on the SLA implant surface at 1,500X (B), 2,000X (D), 5,000X (F), 10,000X (H) of magnification. White arrows in H show the characteristic morphology of bacteria embedded in exopolysaccharide matrix.



**Figure 5.** SEM images and EDX compositional mapping of Laser implant surface (A – C) and SLA implant surface (F – E) after 28 days of incubation in SBF at 37°C. Images were taken at 1,100X and 1,400X of magnification.

high antibacterial activity against a representative peri-implant bacterium as compared to the SLA implant. The reduced number of bacteria grown on the Laser - textured implant surface was verified by counting of viable bacteria and through of SEM observations. The smoother surface of

Laser implant significantly decreases the bacterial attachment and biofilm formation on the implant. The biofilm formation on implant surface strongly depends on the previous adsorption of water molecules and proteins<sup>(15)</sup>, which promote the bacterial colonization. In the current study, Laser - designed implant surface exhibited a lower protein adsorption capacity as compared to the SLA. These results indicate that lower free energy provided by the smooth Laser surface decreases the protein attachment and consequently, the biofilm formation. In contrast, the irregularities of the rough SLA implant surface promote higher protein adsorption, which facilitates the biofilm establishment. Although smooth implant surfaces have been suggested for resisting bacterial colonization<sup>(16)</sup>, this effect have been scantily verified on commercial dental implants fabricated with Laser texturing technology. Uhlman et al.<sup>(17)</sup> detected with crystal violet staining a reduced attachment of *Streptococcus mutans* on laser microtextured titanium surfaces. Zwahr et al.<sup>(18)</sup> used laser processing to produce hierarchical patterns on titanium sheets, which were able to reduce the adherence of *Escherichia coli*. Ionescu et al.<sup>(19)</sup> studied a laser-designed titanium surface regularly formed by 18 - 20 µm micropits, which shown to reduce the formation of a nonspecific biofilm from saliva. Therefore, most of the reported studies on Laser surfaces did not consider specific peri-implant pathogens such as *Porphyromonas gingivalis* or *A. Actinomycetemcomitans*. Lasserre et al.<sup>(20)</sup> found that these bacteria present similar frequency in both peri-implantitis and periodontitis conditions. Although the antimicrobial capacity of the Laser - treated implants strongly will depend on the structural characteristics generated on its surface, *in vitro* antibacterial properties of the Laser implant found in the current study could contribute to reducing the probabilities of infection. Our study also had some limitations. Antibacterial activity of the implant surfaces was measured by using a single bacteria biofilm model, however peri-implant microbiome has been characterized by 71 species, with 12 of them enriched in peri-implantitis diseased sites<sup>(21)</sup>. So, further studies could be performed by using multibacteria biofilms models. In addition, antibacterial effectiveness of the Laser-textured implant surface should be confirmed through both *in vivo* animal testing and clinical trials.

On the other hand, no mineralization of bone-like apatite was detected on the implant surfaces by using the standard acellular SBF assay. Therefore, the micro- and nano-scale analysis of the osseointegration properties of the Laser implant would require further *in vitro* and *in vivo* biological experiments, including cell differentiation assays and animal models.

## CONCLUSIONS

The dental implant fabricated by laser texturing technology is constituted by regular and smooth surface topography. The smooth Laser - treated surface exhibits antibacterial properties that decrease the growth of bacterial biofilm, which was found to be associated with a reduced adsorption capacity of bacterial adhesion proteins. Thus, the Laser implant could contribute to decrease the risk of dental peri-implant infection.

## CLINICAL RELEVANCE

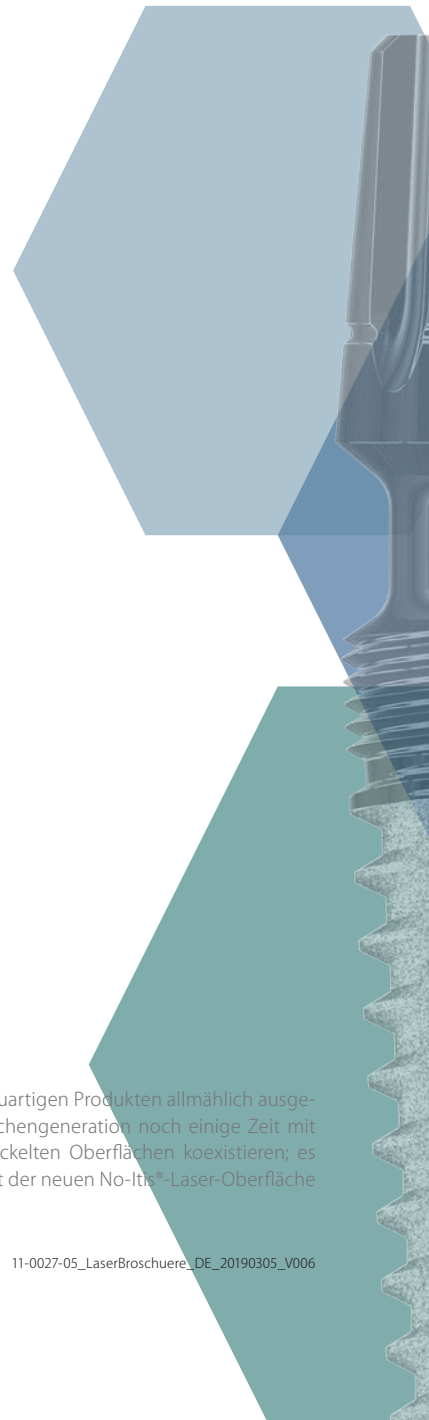
The current study compares the structural and antibacterial properties of a Laser - treated commercial dental implant (No-Itis®) with those of a traditional sandblasted and acid-etched (SLA) implant. The results demonstrated that implant with Laser - treated has a regular and smooth titanium surface that significantly reduce the bacterial growth as compared with that of a traditional SLA implant. These findings suggest that the antibacterial properties exhibited by the dental implant with smooth Laser-designed surface could contribute to reduce the risk of peri-implant infection, which is one of the main reasons of dental implant failure.

## CONFLICT OF INTERESTS.

The authors declare that they have no conflict of interest.

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